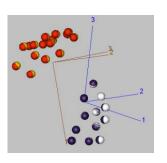




Biomechanical Modelling Applied to Human Movement Analysis



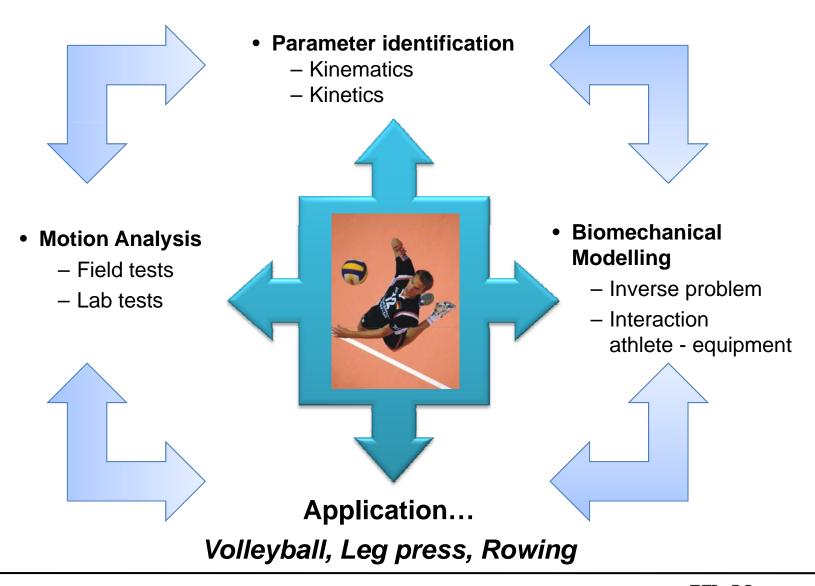




Karen Roemer PhD
Dept. Exercise Science, Health and Physical Education
Michigan Technological University



General Idea...





- Biomechanical Modeling
 - Shoulder kinematics



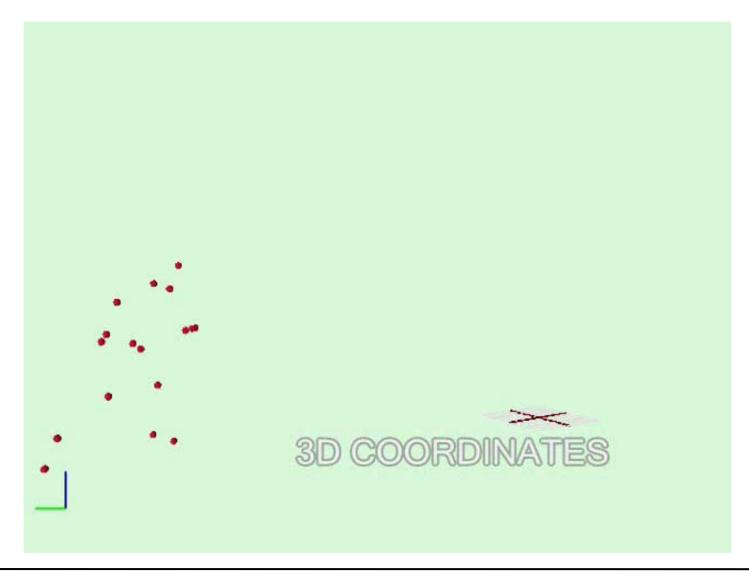
- 3D Motion Analysis
 - Field test

Application

Investigation of shoulder angles in volleyball spikes









- Analysis of shoulder kinematics for volleyball spikes
- Definition of parameters for the investigation of shoulder kinematics in volleyball spikes
- Definition of parameters and graphs to present the results to coaches
- Focus on the phase between strike out position and ball impact



- Pilot study with 2 subjects and 4 spikes
- Follow up study with 10 subjects and 16 spikes



Data Acquisition:

 European top level outside hitters of the national teams of Croatia, Estonia, Germany, and Netherlands



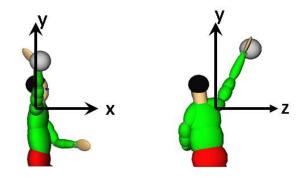
- European League
- Pilot study: four high speed Basler cameras (100Hz) and the software Simi Motion
- Follow-up study: eight high speed Basler cameras (200Hz), two Vosskuehler (200-1000Hz) and the software Simi Motion
- Manual digitizing
- Reproduction of movements with high accuracy (control points: ± 9 mm) using the man model DYNAMICUS (Roemer et al. 2007).



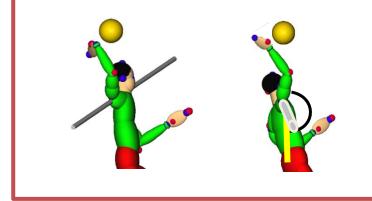
Data Processing:

• time normalization with respect to take-off and ball-impact

position and orientation of the coordinate systems fixed to thorax and humerus were defined using the ISB recommendations



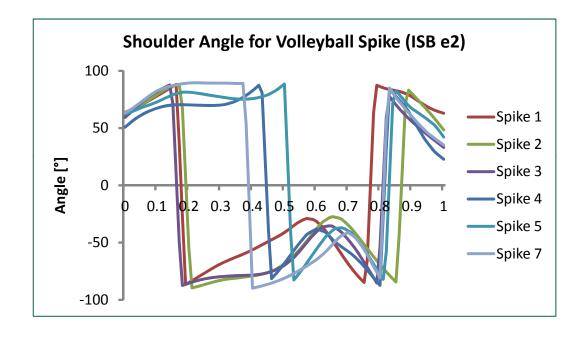
Based on the unit quaternion, the axis angle representation of this rotational movement was determined (Liu & Prakash 2003)





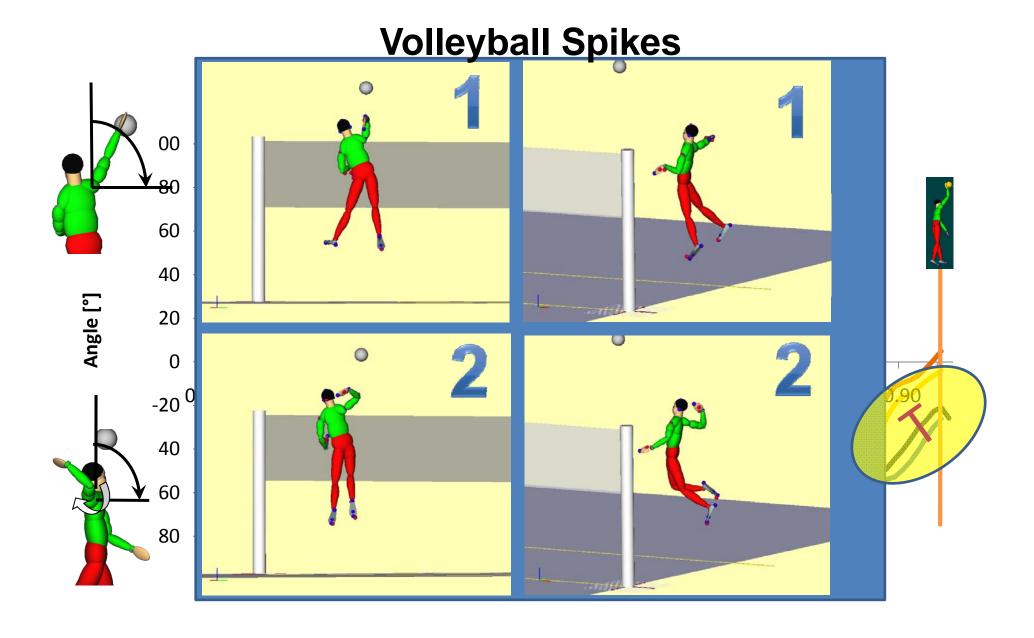
Euler angles lead to discontinuities in time histories of results → gimbal lock (GL)

 ISB shoulder group proposed standardization for describing shoulder kinematics (Wu et al. 2005)

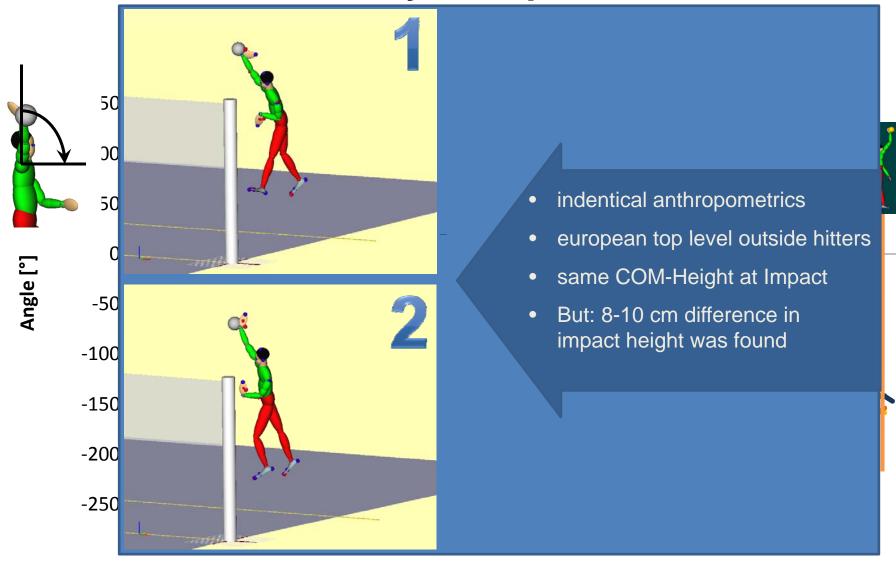


- Depending on the observed range of motion other rotation sequences can be found in the literature to avoid the GL (Levasseur et al. 2007, Senk & Cheze 2006)
- altering the rotational sequence influences results significantly (Karduna et al. 2000)



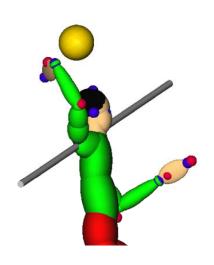






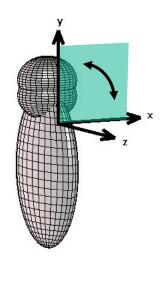


	Trial 1	Trial 2	Trial 3	Trial 4	Trial 5	Trial 6	Trial 7	Trial 8	Trial 9	Trial 10	Trial 11	Trial 12	Trial 13	Trial 14	Trial 15	Trial 16
ellb x-coord./ axis z-coord.	-0.94	-0.98	-0.99	-0.95	-0.80	-0.79	-0.81	-0.78	-0.70	-0.98	-0.85	-0.97	-0.84	-0.99	-0.95	-0.94
ellb y-coord./ axis z-coord.	-0.98	-0.97	-0.94	-0.91	-0.78	-0.82	-0.84	-0.92	-0.97	-0.95	-0.64	-0.93	-0.62	-0.95	-0.97	-0.98



→ movements in the sagittal plane influence the orientation of RA concerning
 z-coordinate significantly (p<0.01)

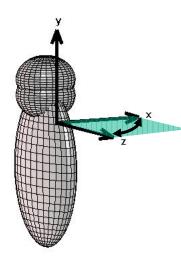




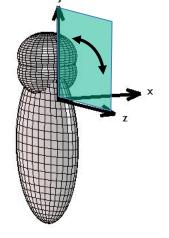


Trial 1 Trial 2 Trial 3 Trial 4 Trial 5 Trial 6 Trial 7 Trial 8 Trial 9 Trial 10 Trial 11 Trial 12 Trial 13 Trial 14 Trial 15 Trial 16



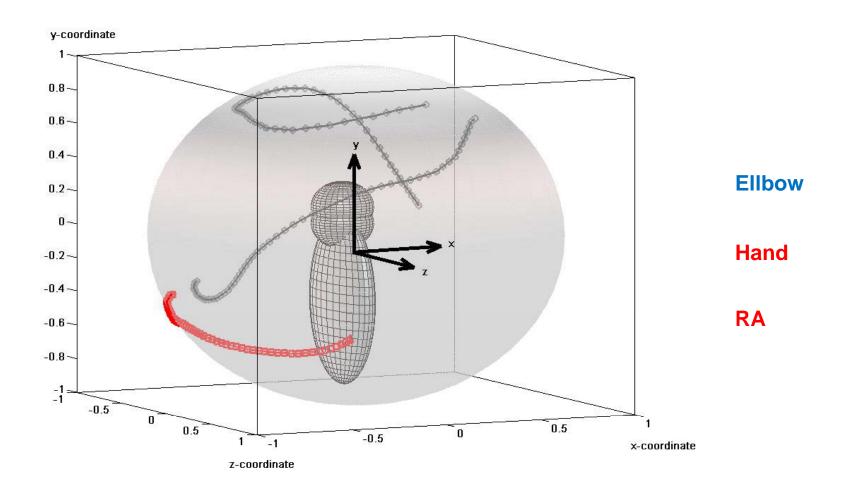


- eight trials out of 16 show no significant correlation
- → four trials indicate significant positive correlation
- → four trials indicate significant negative correlation for the same coordinate

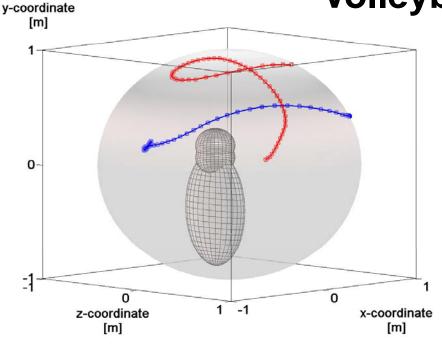


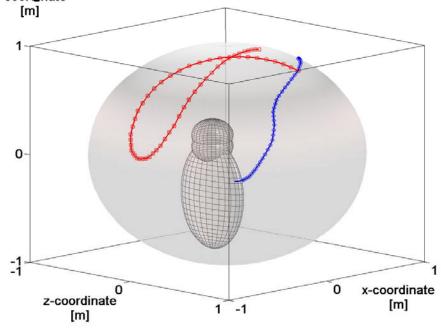












ROM: 90° to 142°

Start: min. 60° of internal rotation

→ Changes in the elbow z-coordinate do correlate with rotational angles in the shoulder joint

→ Negative correlation of elbow z-coordinate with RA x coordinate

ROM: 53° to 116°

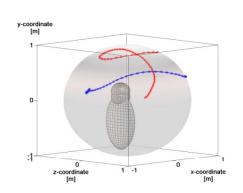
Start: max. 50° of internal rotation

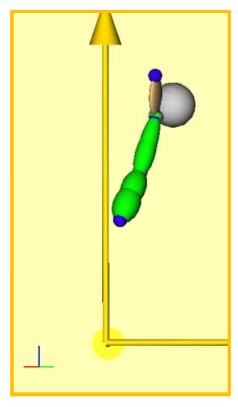
→ Changes in the elbow z-coordinate do not correlate with rotational angles in the shoulder joint

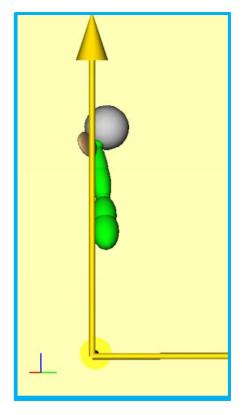
→ Positive correlation of elbow zcoordinate with RA x coordinate

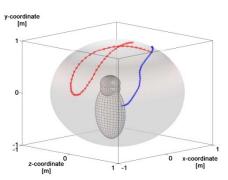


Impact-Indicator







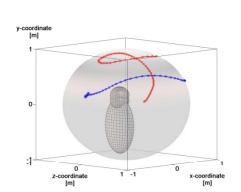


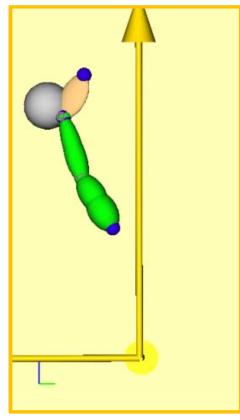
Technique 1

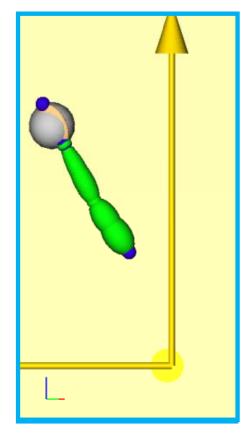
Technique 2

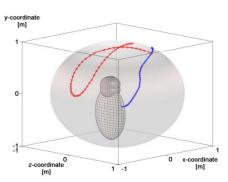


Ball-Indicator







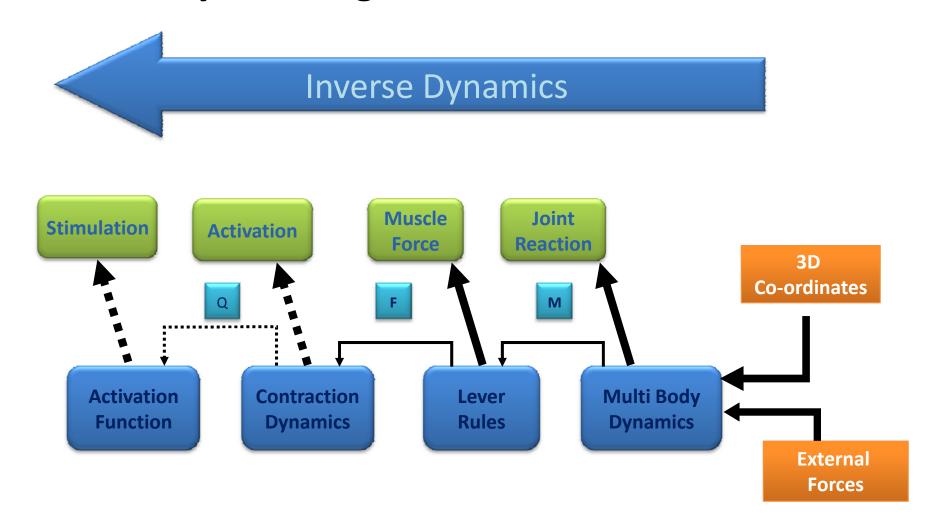


Technique 1

Technique 2

→ Graphic representation of results to transfer the knowledge to athletes and coaches

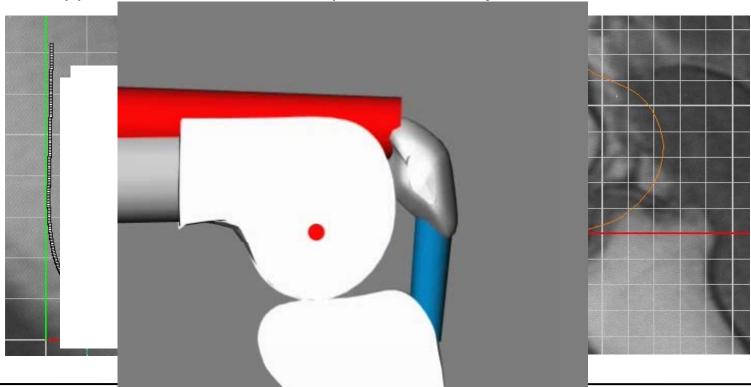




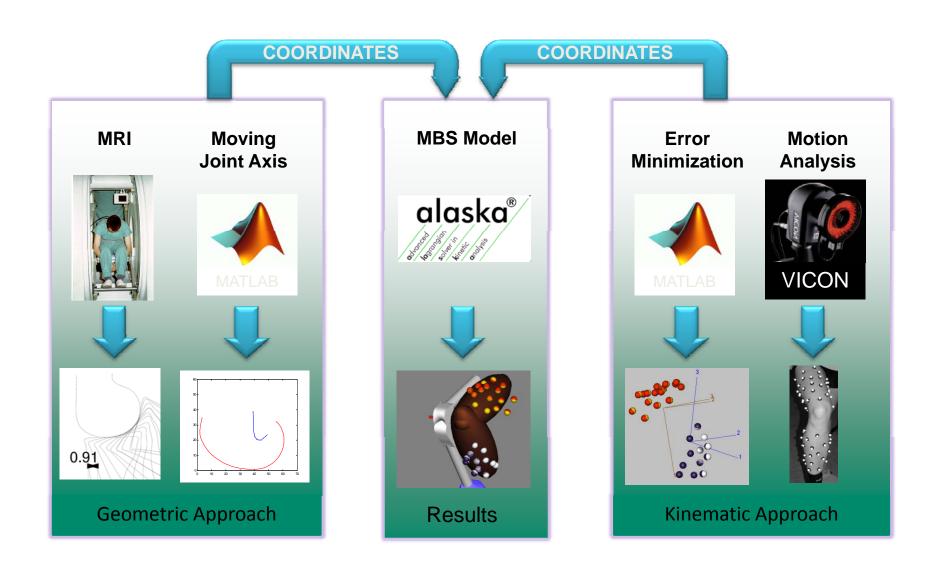


Geometric approach

- MRI based model, coordinates of joint axis depend on the outline of the condylus femoris
- and the linear displacement of the tibia (see WANK 2000)
- applied to tibio-femoral and patello-femoral joint

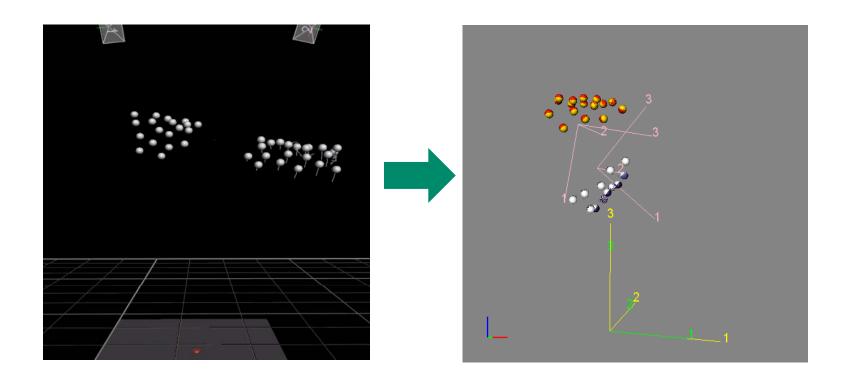






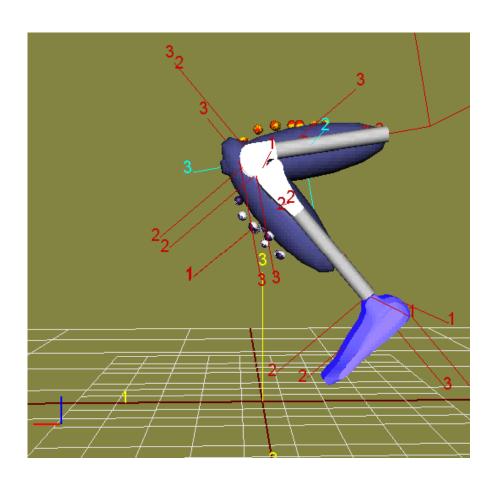


Kinematic Theory Approach (Motion Analysis)



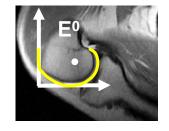


MBS Model

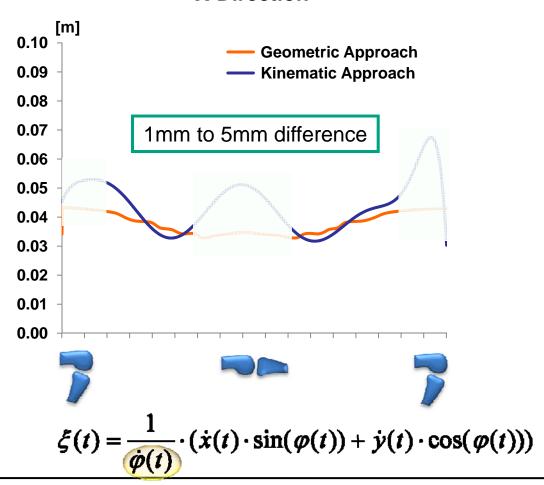




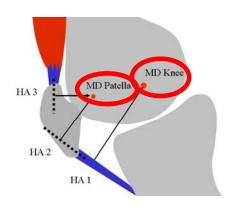
Femur related results



X-Direction



Influence of different model types on calculated muscle forces



- Individually parameterized models for:
 - tibiofemoral joint with moving joint axis
 - patellofemoral joint with moving joint axis

- → Tibiofemoral joint as hinge joint
- → Patellofemoral joint moving on a circular path

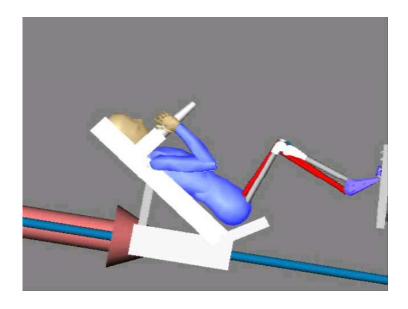
- → Individually parameterized with a moving joint axis
- → Individually parameterized path for the patella with a moving joint axis



Reconstruction of the movement

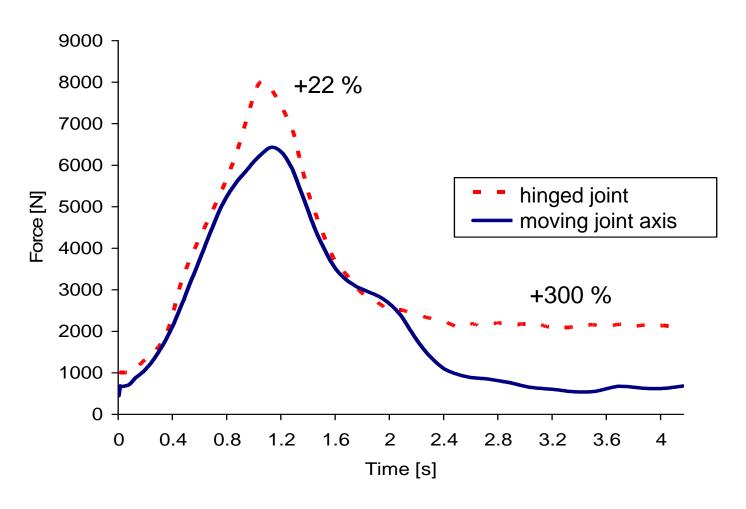
- Integration of the Lagrangian equations of motion using alaska
- Calculation of time histories for the spatial coordinates of the man model DYNAMICUS





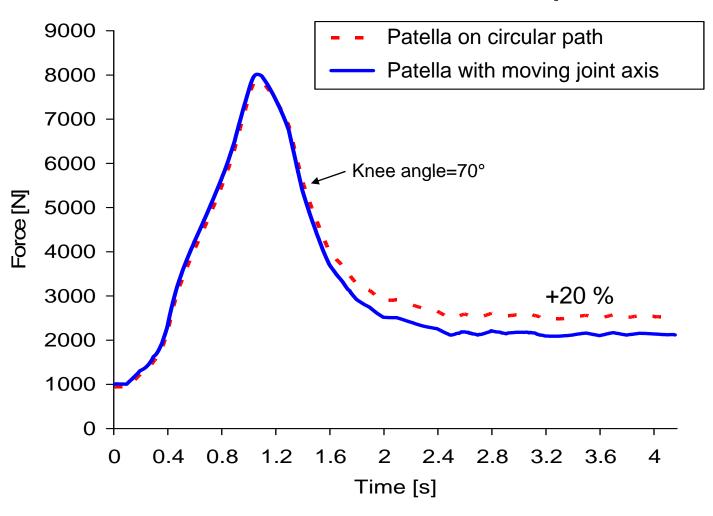


Force of Mm. Quadriceps



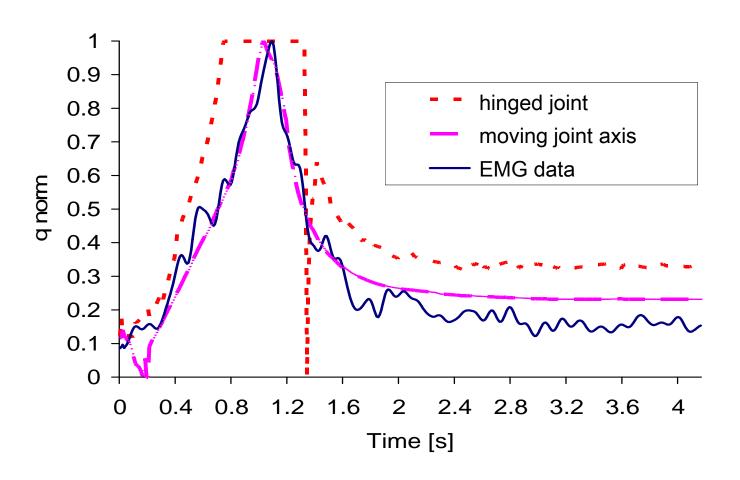


Force of Mm. Quadriceps

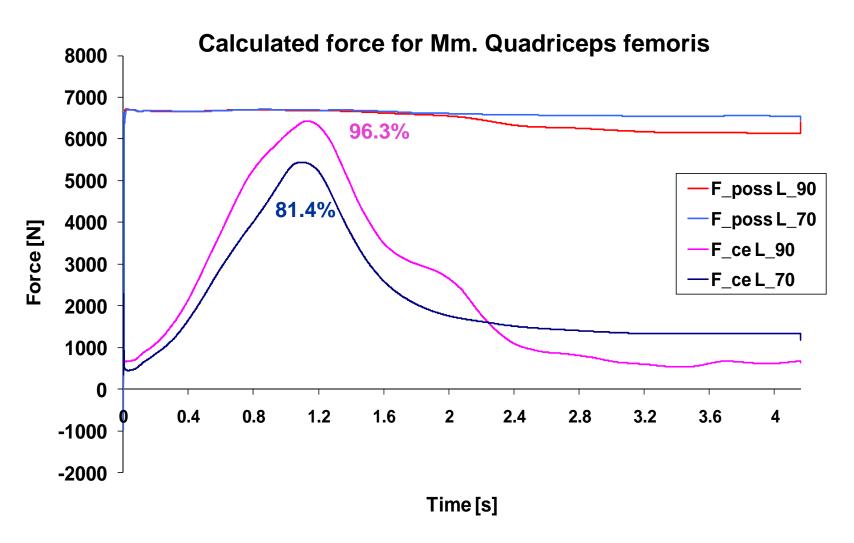




Stimulationfunction





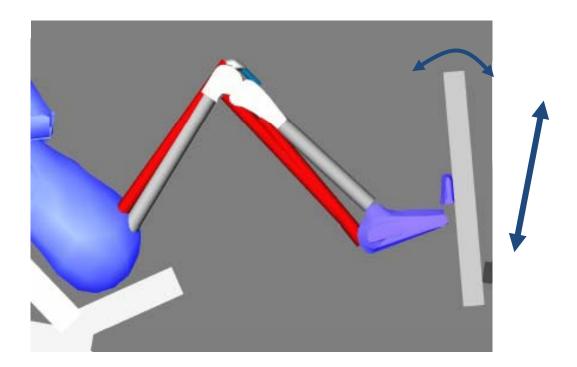


→ How can we match the internal load with the external load?

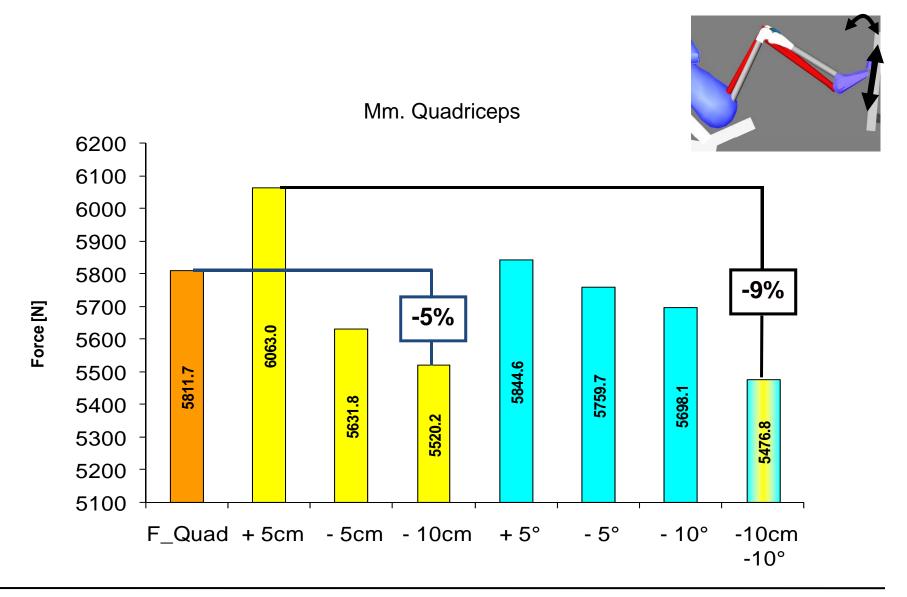


The following boundary conditions were varied:

- Contact position on the foot pad: +5 cm, -5 cm, -10 cm
- Angle of the foot pad: +5 °, -5 °, -10 °.

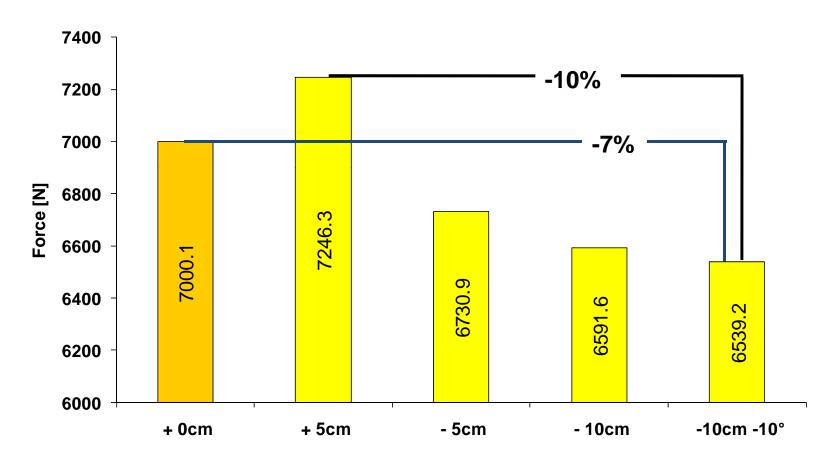






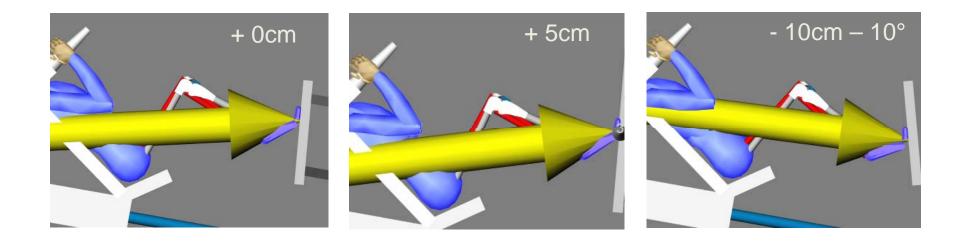


Force between Patella and Femur Condyle





Reason: Orientation of the GRF



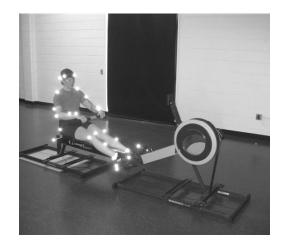
→ Graphic representation of results to transfer the knowledge to athletes, coaches, and PT



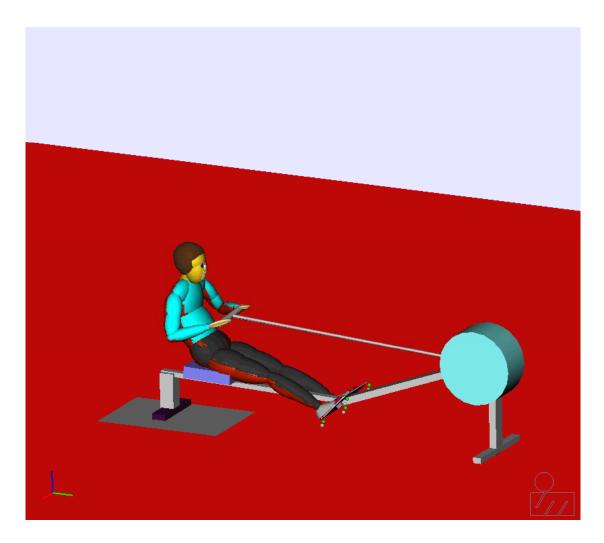
- 40 subjects
 - →10 NW skilled
 - →10 NW
 - →10 overweight
 - →10 obese

Height [cm]	Age [y]	BMI [kg/m²]				
179±9	23±4	21.9±1.2				
174±8	27±7	21.8±1.6				
171±9	24±6	26.7±1.3				
170±9	26±3	35.5±4.7				

rowing at three different resistance levels for 2 min each → 2min rest

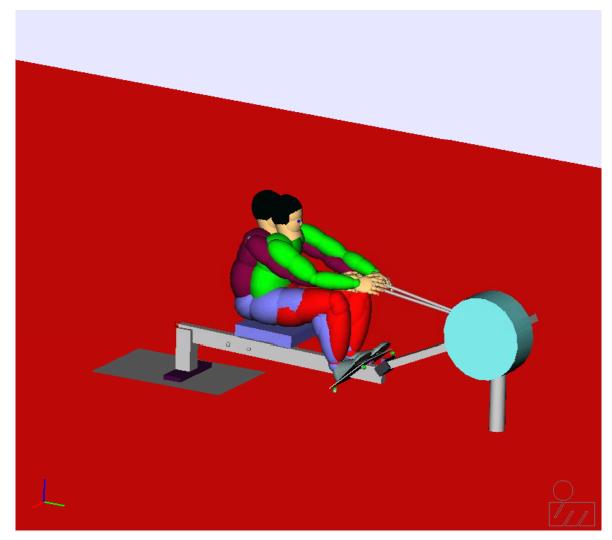






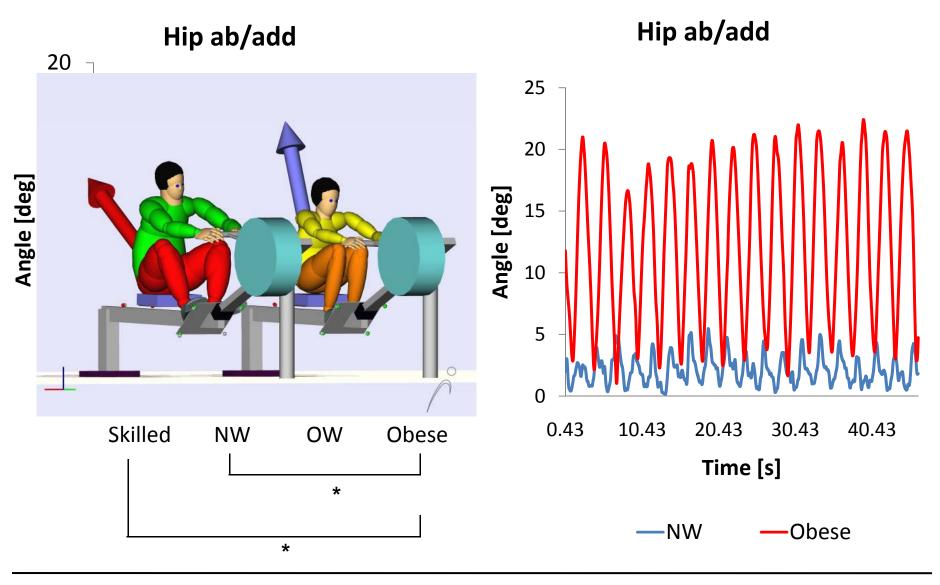
Within subject variability: ±0.9° for 10 strokes



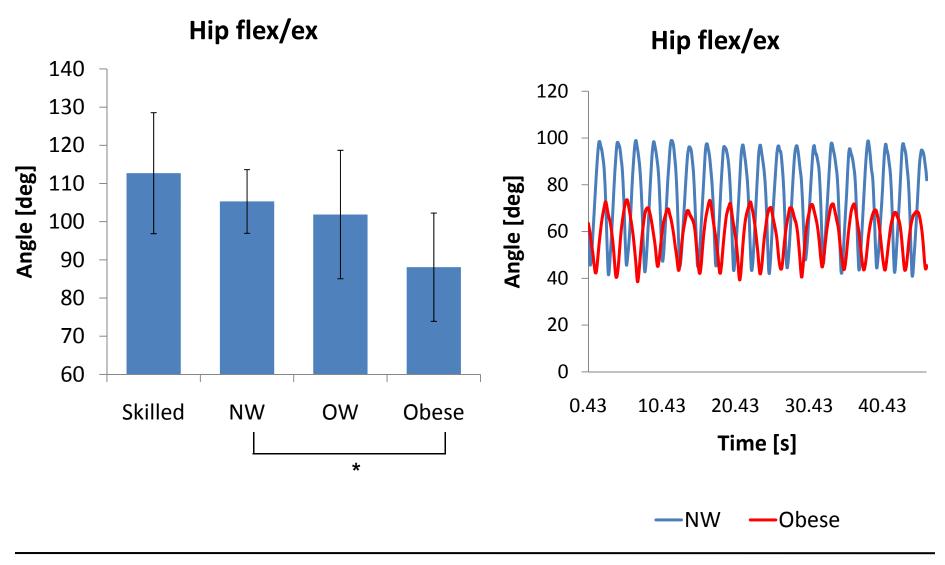


Within subject variability: ±0.9° for 10 strokes

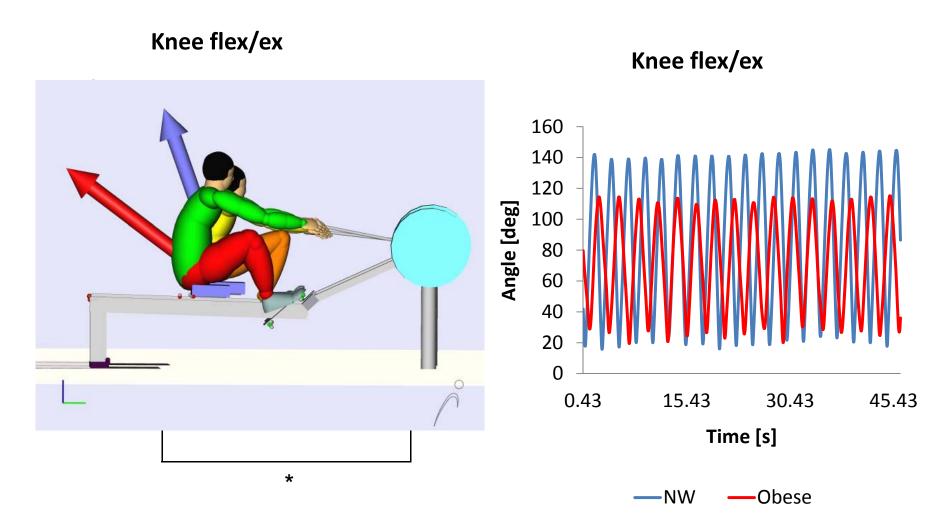








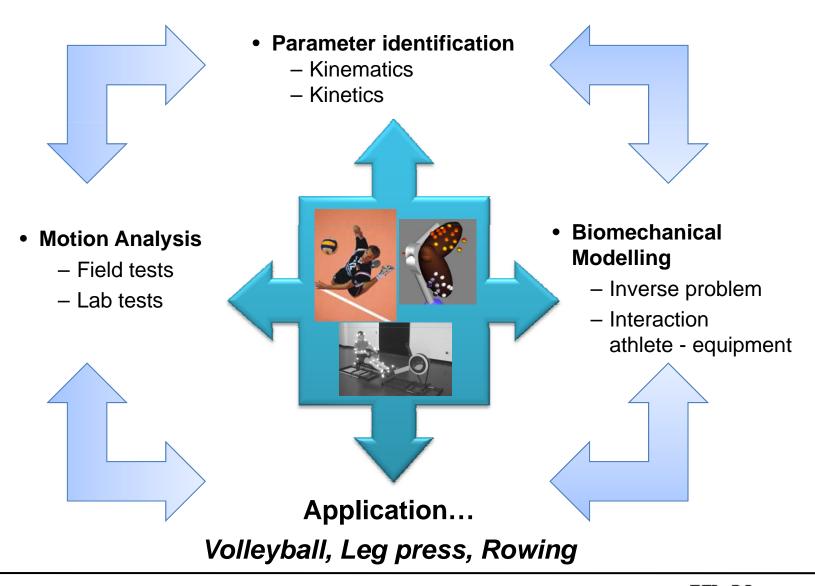




→ Graphic representation of results to transfer the knowledge to athletes, coaches, and PT



General Idea...





Application ...

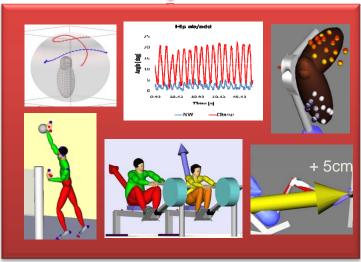
- Parameter identification
 - Kinematics
 - Kinetics

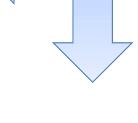




- Field tests
- Lab tests







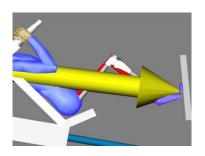
- Biomechanical Modelling
 - Inverse problem
 - Interaction athlete - equipment



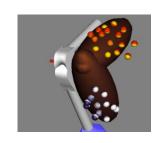
Transfer

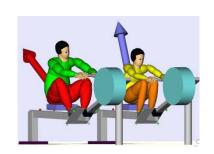
Coaches, Athletes, Students





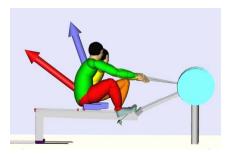




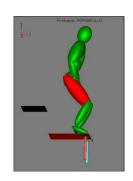


Thank you for your attention









Acknowledgements:

Claas Kuhlmann, Frank Lindner Chemnitz, University of Technology, Germany Stephanie Hamilton, Chris Richter, Michigan Technological University, USA

